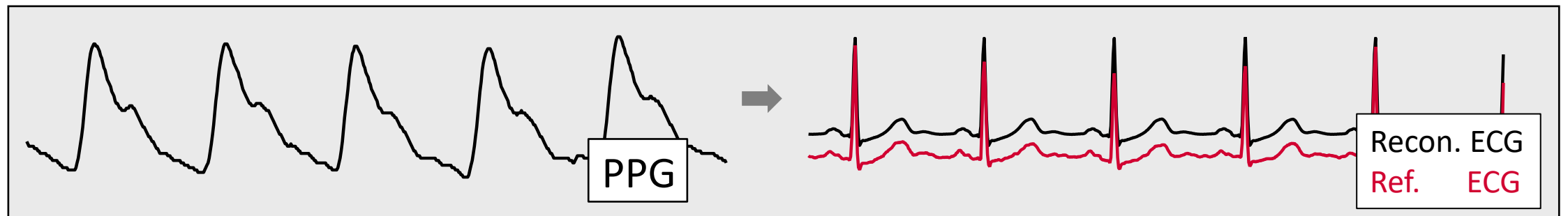


# Learning Your Heart Actions From Pulse: ECG Waveform Reconstruction From PPG

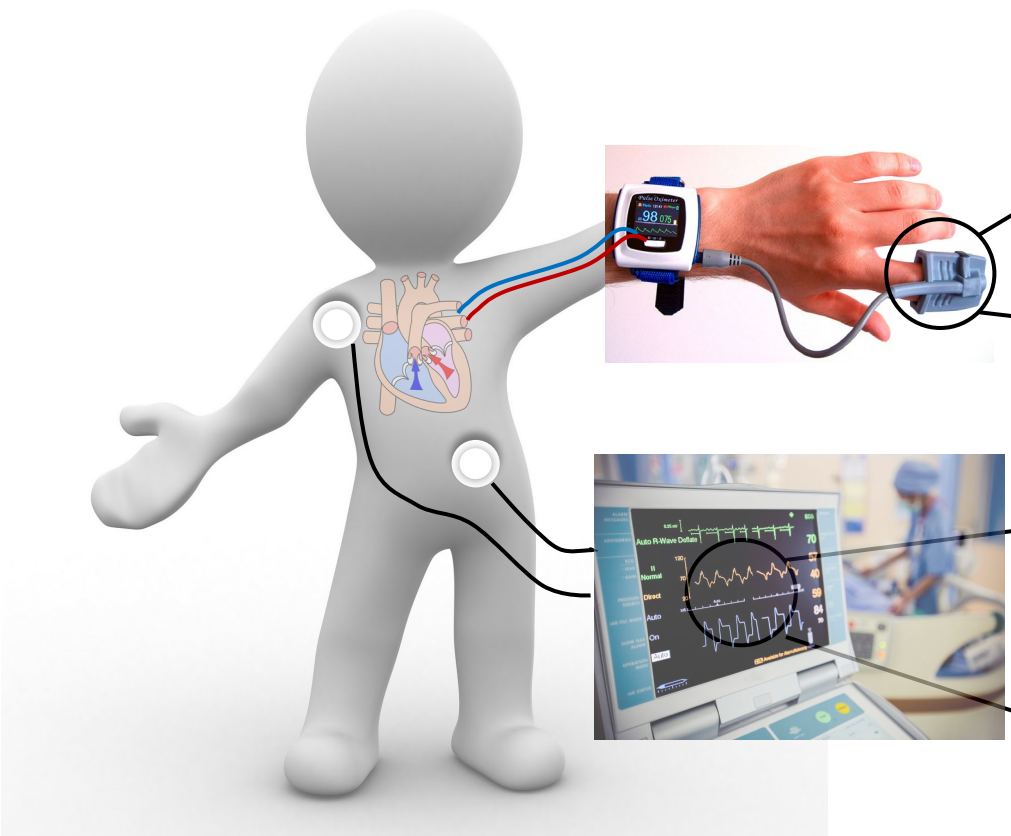
Qiang Zhu<sup>1</sup>, Xin Tian<sup>1</sup>, Chau-Wai Wong<sup>2</sup>, and Min Wu<sup>1</sup>

<sup>1</sup> Electrical and Computer Engineering, University of Maryland, College Park

<sup>2</sup> Electrical and Computer Engineering, North Carolina State University

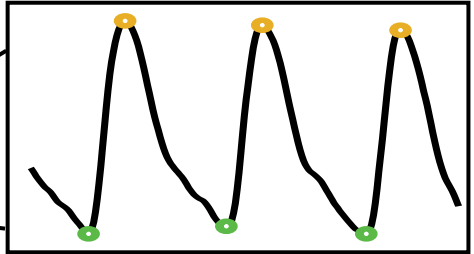


# Continuous Cardiovascular Monitoring: ECG vs. PPG — Pros and Cons



## PPG

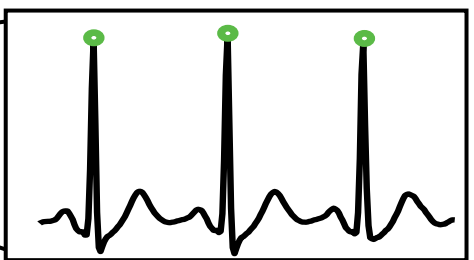
Photoplethysmogram



Optical sensing

Less direct cardiac information

More user-friendly and cheaper



## ECG

Electrocardiogram

Bio-electrical signal

Clinical gold standard

Restrictive; uncomfortable

# ECG from PPG — Benefits and Research Problems



Knowledge  
Base



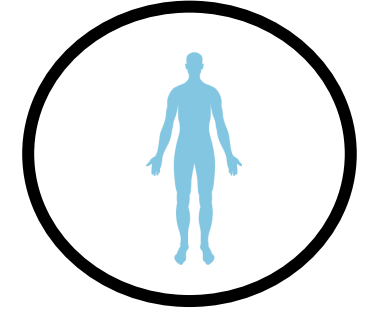
Low  
Cost



Continuous  
Real-time



User  
Friendly



Digital Twins  
Monitoring

*Two major research problems:*

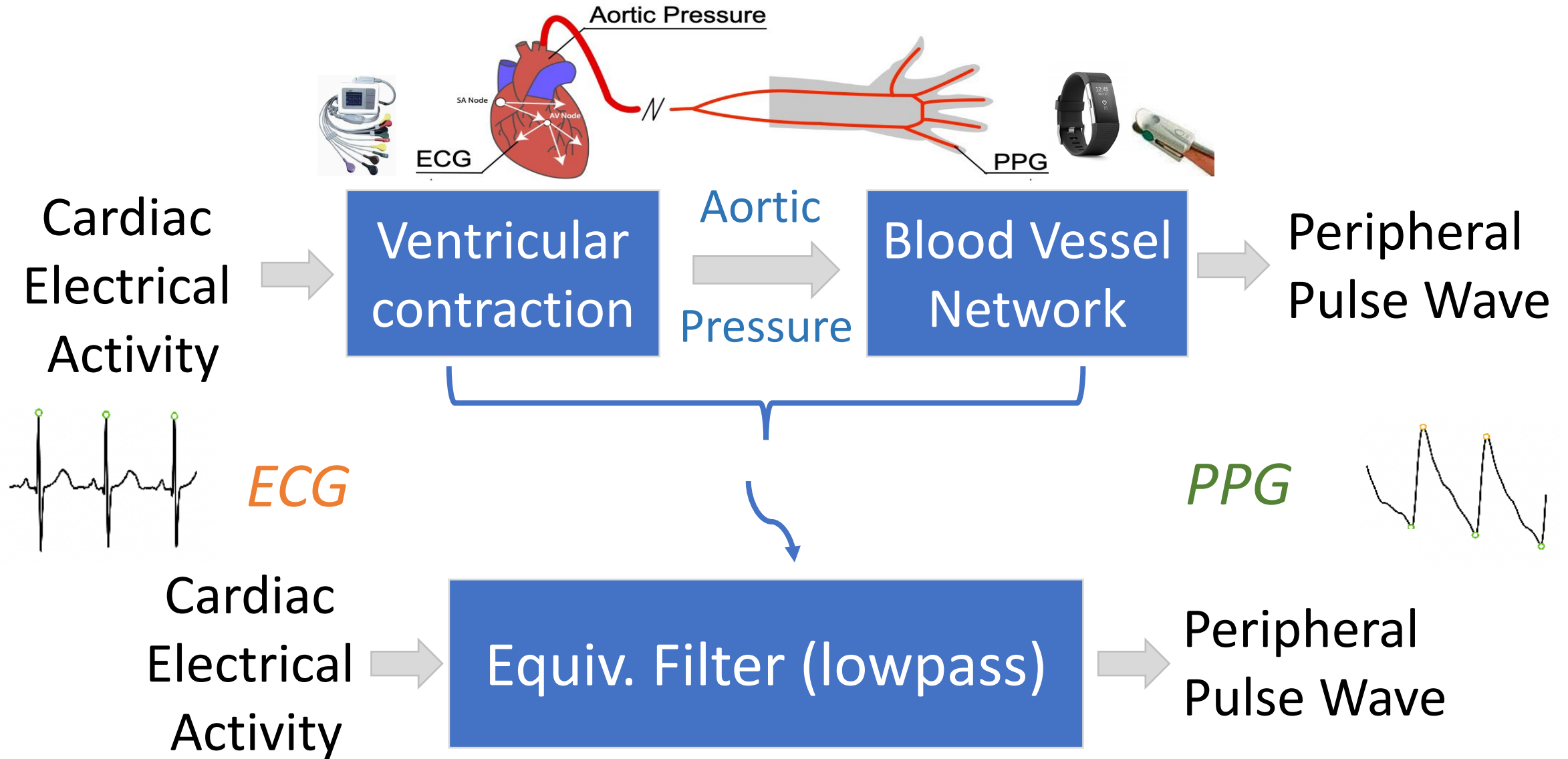
1. Infer ECG from *clean* PPG?

Fundamental  
& our focus

2. Clean up noisy PPG due to movement etc.?

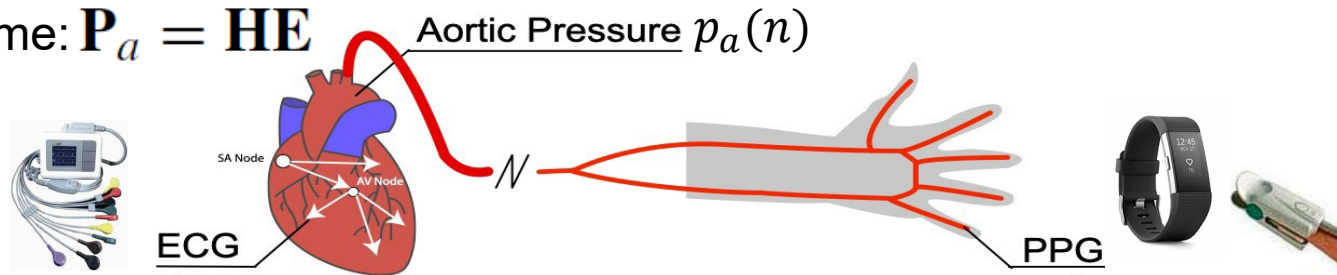
- Leverage multiple sensors (e.g., accelerometers)

# A Signal Model between ECG and PPG



# Characterize the Signal Model Between ECG and PPG

Assume:  $\mathbf{P}_a = \mathbf{H}\mathbf{E}$



$$\text{ECG: } c_y(n) = \alpha e(n) + v_y(n)$$

- $e(n)$ : Myocardial activities
- $\alpha$ : Human body resistance of the electrical path from the heart to the skin surface;
- $v_y(n)$ : ECG sensor noise.

$$p_p(n) = b(n) \otimes p_a(n) + v_b(n)$$

$$\mathbf{P}_p = \mathbf{B}\mathbf{P}_a + \mathbf{V}_b$$

- $b(n)$ : blood vessel as LTI channel;
- $\otimes$ : symmetric convolution operator;
- $p_p(n)$ : peripheral pulse wave;
- $v_b(n)$ : model noise;
- $\mathbf{P}_p, \mathbf{B}, \mathbf{P}_a, \mathbf{V}_b$ : corresp. DCT coeff.

$$\text{PPG: } c_x(n) = I_1 p_p(n) + I_0 + v_x(n)$$

where  $I_1 = I\tau_1$  and  $I_0 = I\tau_0$

- $I$ : intensity of the light source
- $\tau_0, \tau_1$ : transmissive strength and reflective strength of the skin tissue.

Linear model in DCT domain

$$\mathbf{C}_y = \mathbf{F}\mathbf{C}_x + \mathbf{C}_0 + \mathbf{V}$$

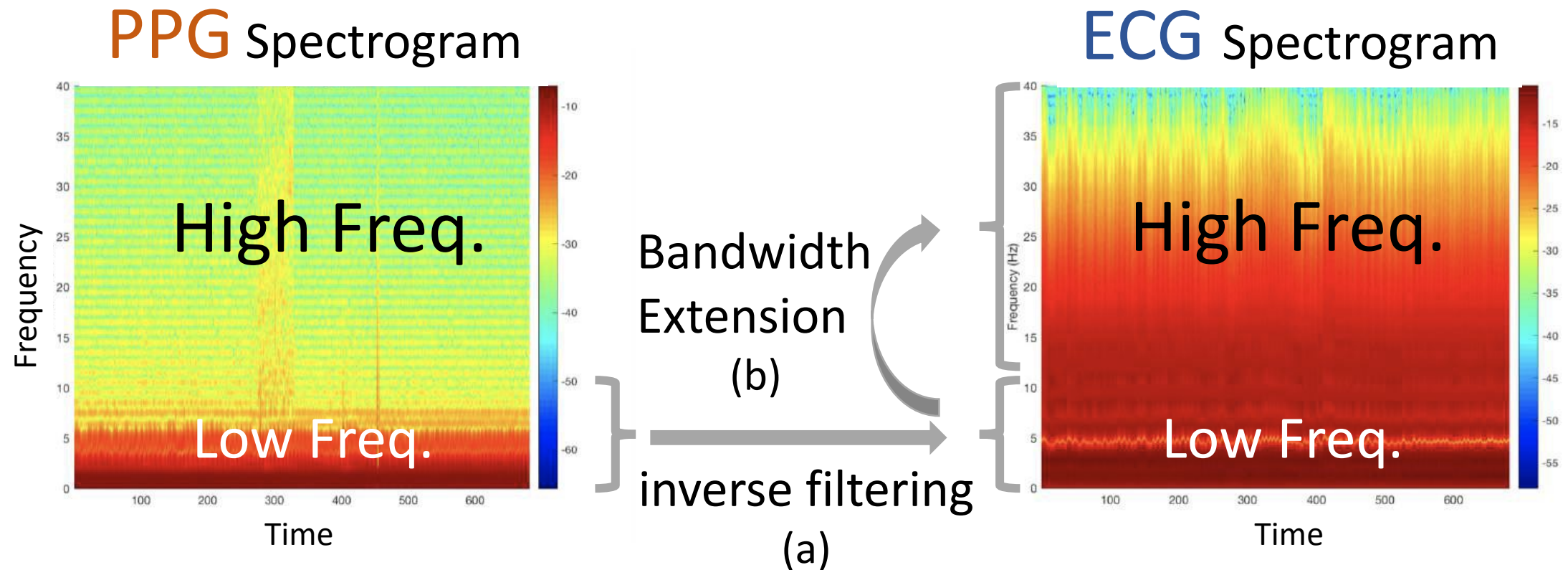
where

$$\mathbf{F} \triangleq \alpha I_1^{-1} \mathbf{H}^{-1} \mathbf{B}^{-1}$$

$$\mathbf{C}_0 \triangleq -\alpha I_1^{-1} \mathbf{H}^{-1} \mathbf{B}^{-1} \mathbf{I}_0$$

$$\mathbf{V} \triangleq \mathbf{V}_y - \alpha \mathbf{H}^{-1} \mathbf{B}^{-1} (I_1^{-1} \mathbf{V}_x + \mathbf{V}_b)$$

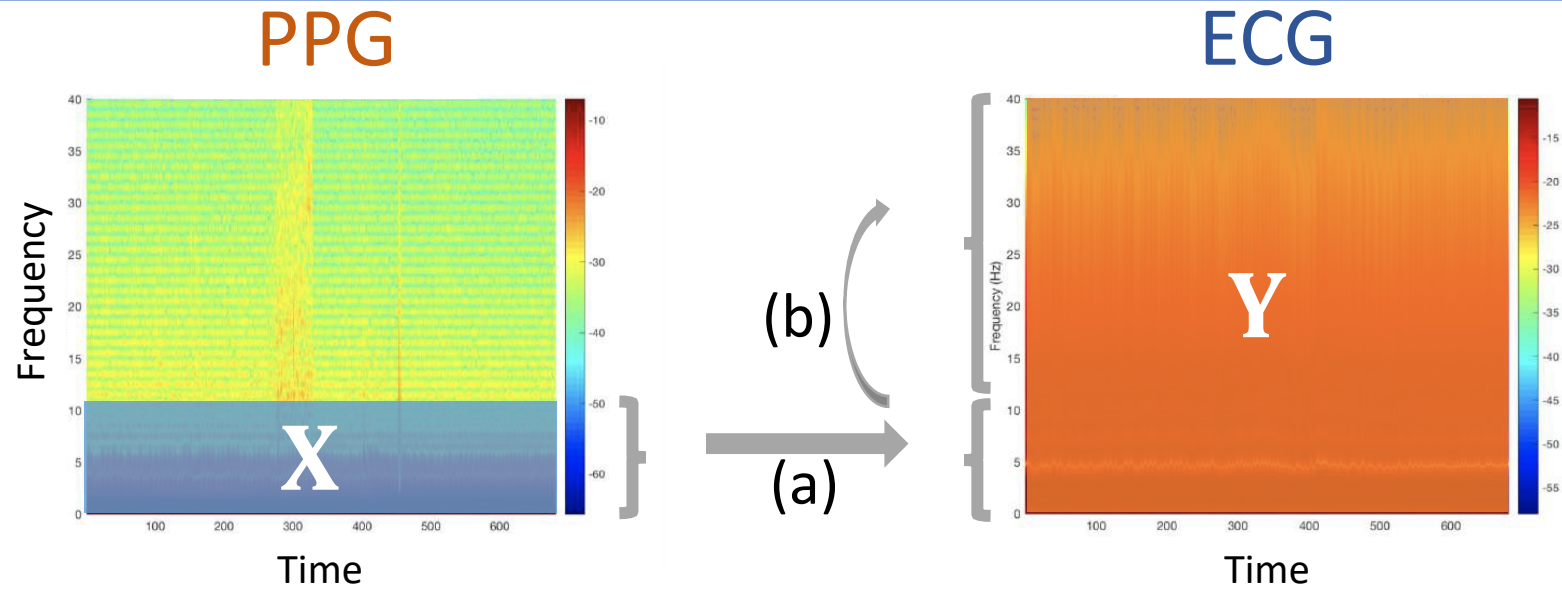
# PPG to ECG: Methodology At-a-Glance



💡 Combine (a) and (b) with *model + data supported learning*

# PPG to ECG: Methodology At-a-Glance (cont.)

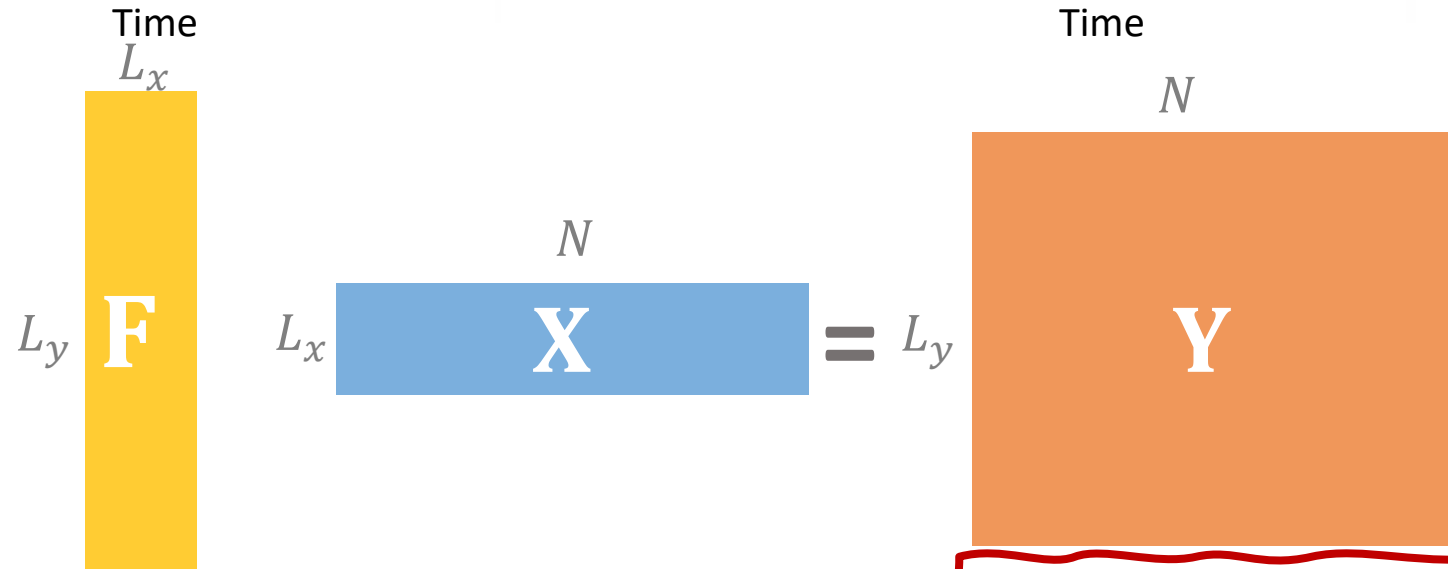
Combine (a) and (b) with model and data learning



Model in freq. domain

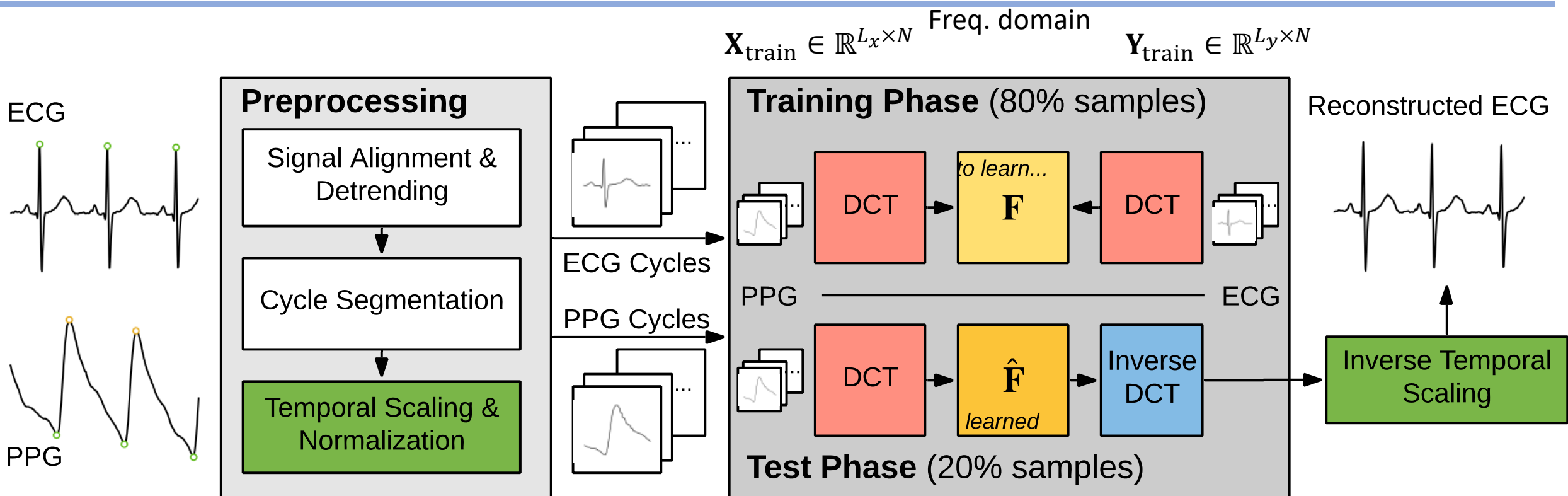
Linear transform  $\mathbf{F}$ :

- $L_x$ : # PPG freq. Coeffi.
- $L_y$ : # ECG freq. Coeffi.
- $N$ : # time indices



Recall: Linear model in DCT domain  $\mathbf{C}_y = \mathbf{F}\mathbf{C}_x + \mathbf{C}_0 + \mathbf{V}$

# A Cycle-based Learning Framework



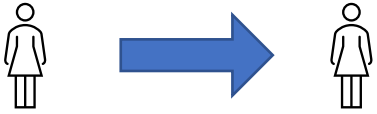
$$\hat{\mathbf{F}} = \underset{\mathbf{F}}{\operatorname{argmin}} \|\mathbf{F}\mathbf{X}_{\text{train}} - \mathbf{Y}_{\text{train}}\|_F^2 + \gamma \|\mathbf{F}\|_F^2$$

A linear transform  $\hat{\mathbf{F}}$  learned by *ridge regression*



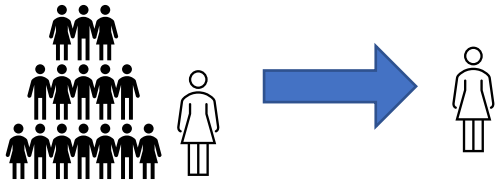
# Subject Specific Model (SM) vs. Group Model (GM)

Two training setups:



## 1. Subject-Specific Model (SM)

Can the proposed learning system, trained by an individual's signal pairs of ECG and PPG, predict his/her ECG waveforms from unseen PPG measurements?



## 2. Group Model (GM)

Can a single model, trained by a group of subjects with certain trait combinations (e.g., age and weight), predict ECG waveforms from unseen PPG measurements for an individual in the training group?

Recall: Linear model in DCT domain

$$\mathbf{C}_y = \mathbf{F}\mathbf{C}_x + \mathbf{C}_0 + \mathbf{V}$$

where

$$\mathbf{F} \triangleq \alpha \mathbf{I}_1^{-1} \mathbf{H}^{-1} \mathbf{B}^{-1}$$
$$\mathbf{C}_0 \triangleq -\alpha \mathbf{I}_1^{-1} \mathbf{H}^{-1} \mathbf{B}^{-1} \mathbf{I}_0$$
$$\mathbf{V} \triangleq \mathbf{V}_y - \alpha \mathbf{H}^{-1} \mathbf{B}^{-1} (\mathbf{I}_1^{-1} \mathbf{V}_x + \mathbf{V}_b)$$

# Datasets for System Evaluation: Diverse Combinations of Age, Weight, and Health Conditions

---

## Capnabase TBME-RR (by UBC, publicly available) [1]

- Collected during elective surgery and routine anesthesia.
- 29 Children and 13 adults (age: min: 1, max: 63, and median: 14; weight: min: 9 kg, max: 145 kg, and median: 49 kg) ).

## Self-Collected UMD Dataset:

- Self-collected data using consumer-grade PPG and ECG sensors.
- Two UMD students participated in this over-two-week data collection.

## Mini-MIMIC (selected data from MIT MIMIC III database [2])

- ICU data with various cardio patients and non-cardio ones.
- 103 patients in total. Each patient has three sessions of 5-min ECG and PPG recordings collected within several hours.

[1]. Karlen, W., Raman, S., Ansermino, J. M., & Dumont, G. A. (2013). Multiparameter Respiratory Rate Estimation from the Photoplethysmogram. *IEEE Transactions on Biomedical Engineering*, 60(7), 1946-1953.

[2]. Johnson, A. E., Pollard, T. J., Shen, L., Li-wei, H. L., Feng, M., Ghassemi, M., ... & Mark, R. G. (2016). MIMIC-III, a freely accessible critical care database. *Scientific data*, 3, 160035.

# Evaluation Methods

Two Evaluation Metrics:

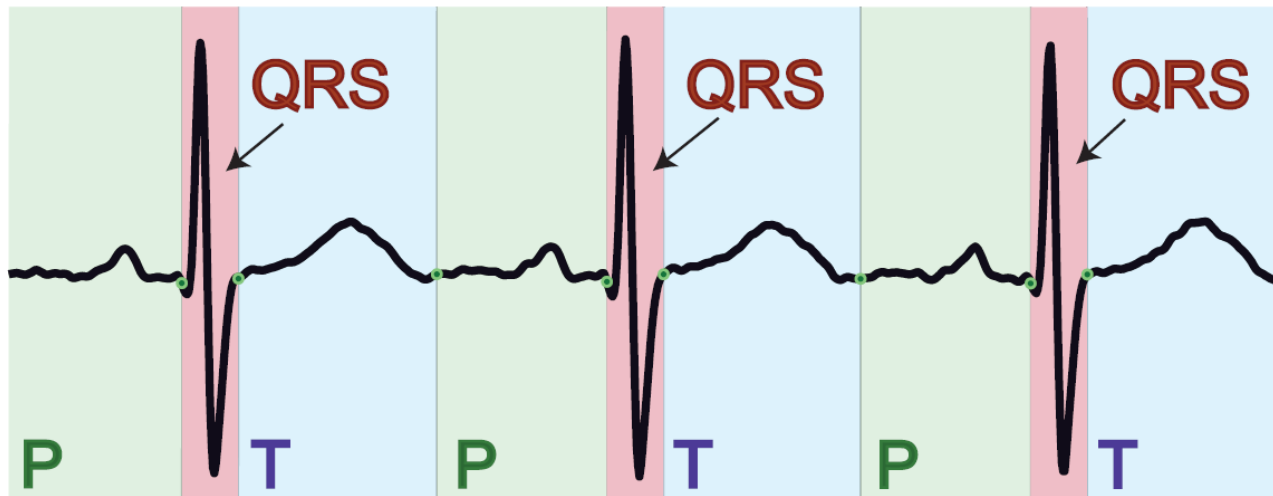
- Relative Root Mean Square Error

$$\text{rRMSE} = \frac{\|\mathbf{y} - \hat{\mathbf{y}}\|_2}{\|\mathbf{y}\|_2}$$

- Pearson's Correlation Coefficient

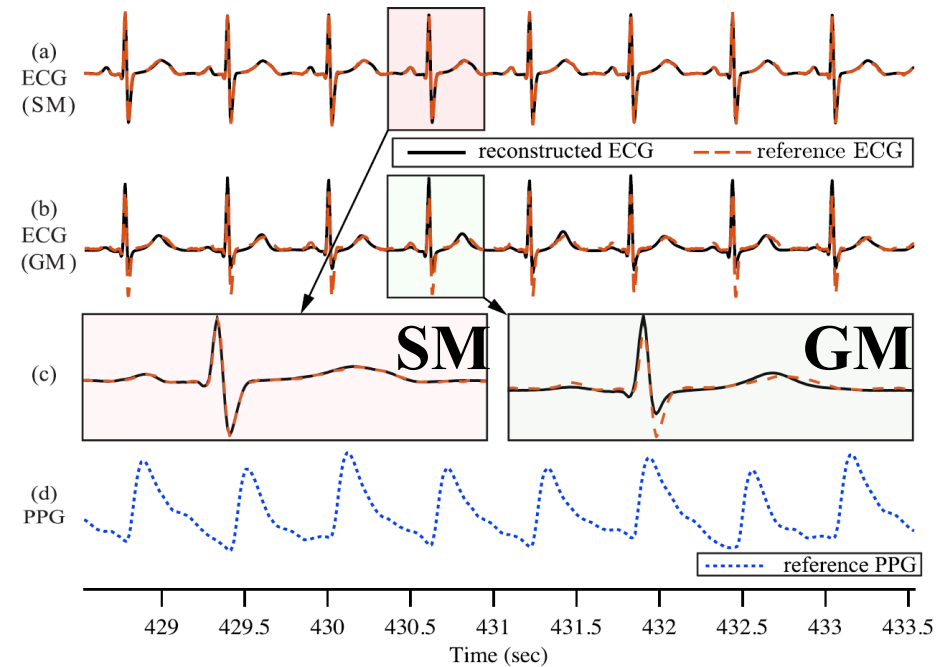
$$\rho = \frac{(\mathbf{y} - \bar{y})^T (\hat{\mathbf{y}} - \bar{\hat{y}})}{\|\mathbf{y} - \bar{y}\|_2 \|\hat{\mathbf{y}} - \bar{\hat{y}}\|_2}$$

Segments Evaluation:



# Evaluation on Dataset 1: TBME-RR dataset

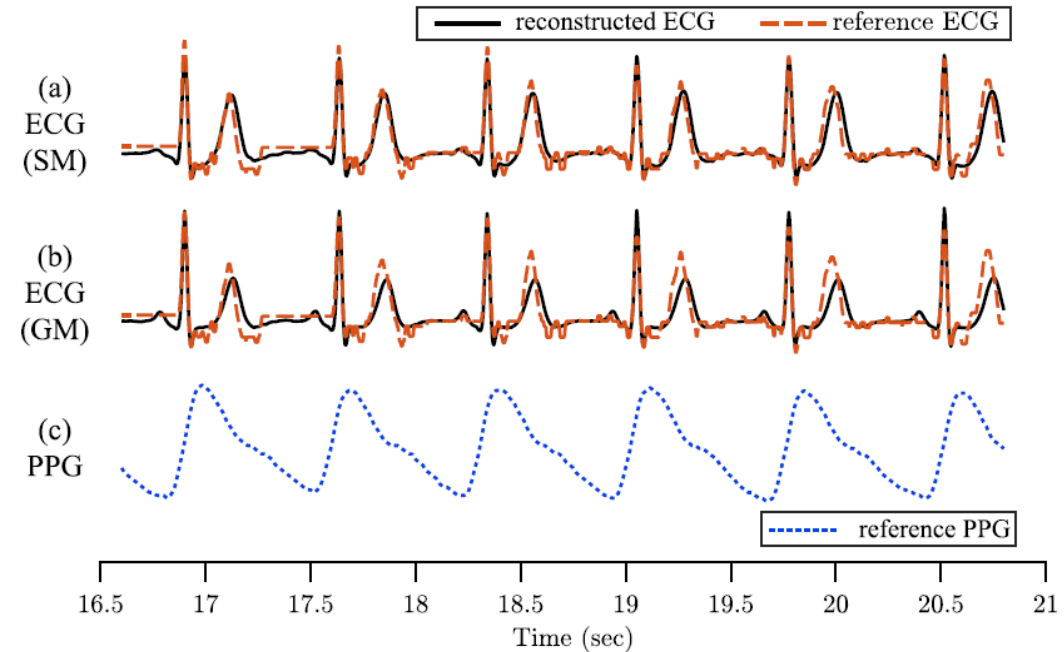
- One example: 4 years old, 18 kg
- Pearson's correlation coeff.  
SM: 0.99  
GM: 0.88
- Overall performance



	Subject Specific Model (SM)				Group Model (GM)			
Average	P	QRS	T	all	P	QRS	T	all
rRMSE	0.27	0.13	0.28	0.17	0.52	0.36	0.72	0.42
$\rho$	0.87	0.99	0.92	<b>0.98</b>	0.69	0.94	0.71	<b>0.91</b>

# Evaluation on Dataset 2: UMD dataset

- One example:
  - Pearson's correlation coeff.  
SM: 0.92  
GM: 0.87



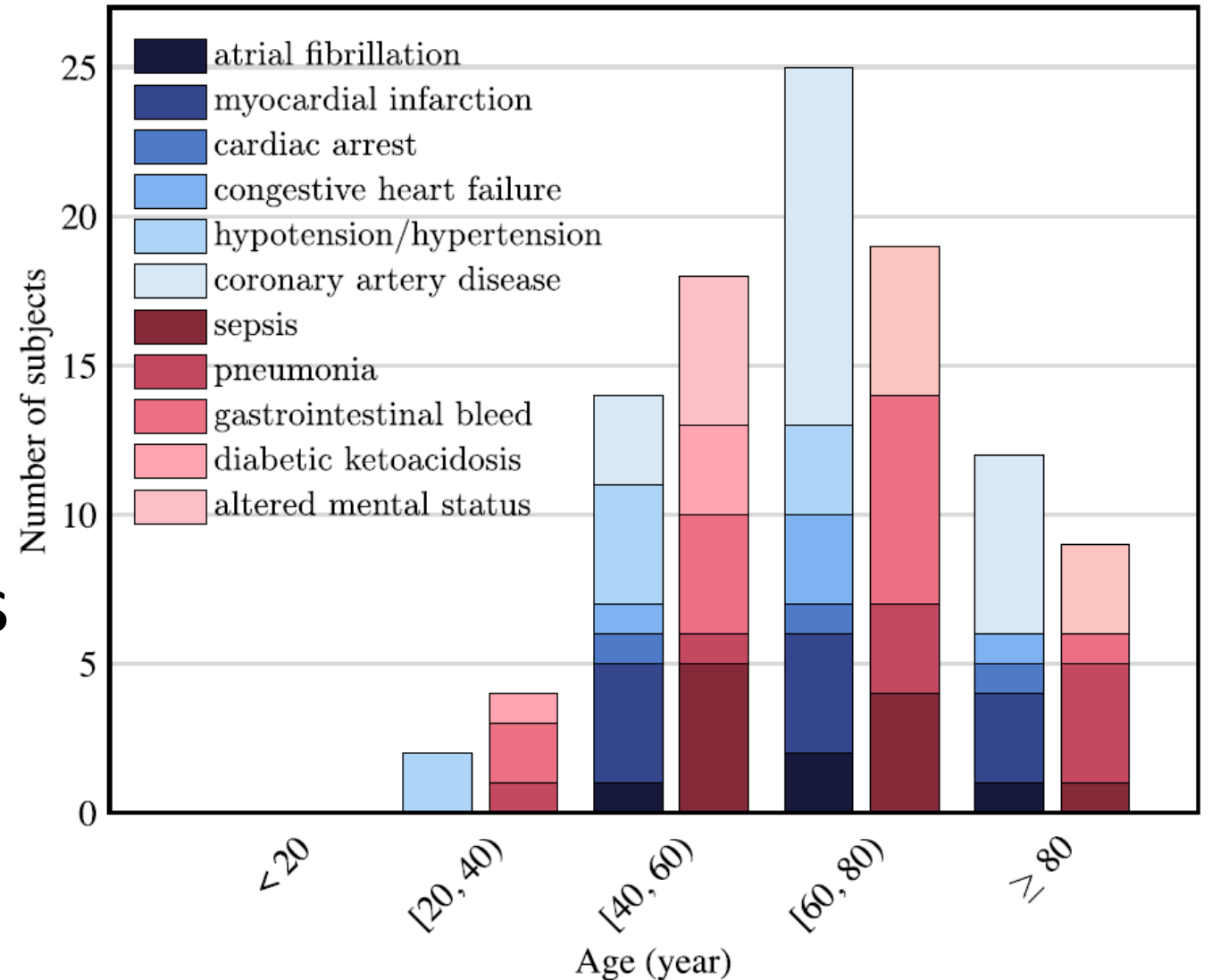
- Overall performance

	Subject Specific Model (SM)				Group Model (GM)			
Average	P	QRS	T	all	P	QRS	T	all
rRMSE	0.66	0.28	0.57	0.43	0.72	0.30	0.59	0.45
$\rho$	0.58	0.97	0.84	<b>0.90</b>	0.50	0.96	0.83	<b>0.89</b>

# Dataset 3: Mini-MIMIC III

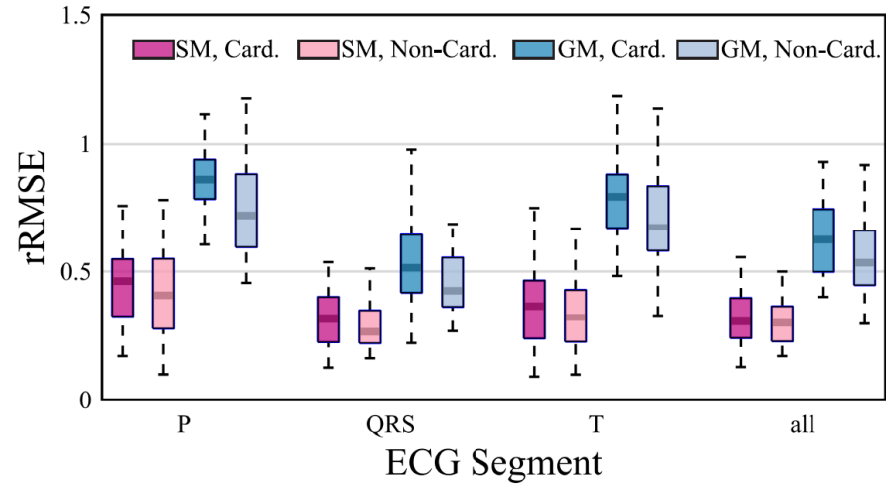
Selected PPG and ECG data from MIMIC III database [2]

- 50 Cardiac Patients
- 53 Non-cardiac Patients

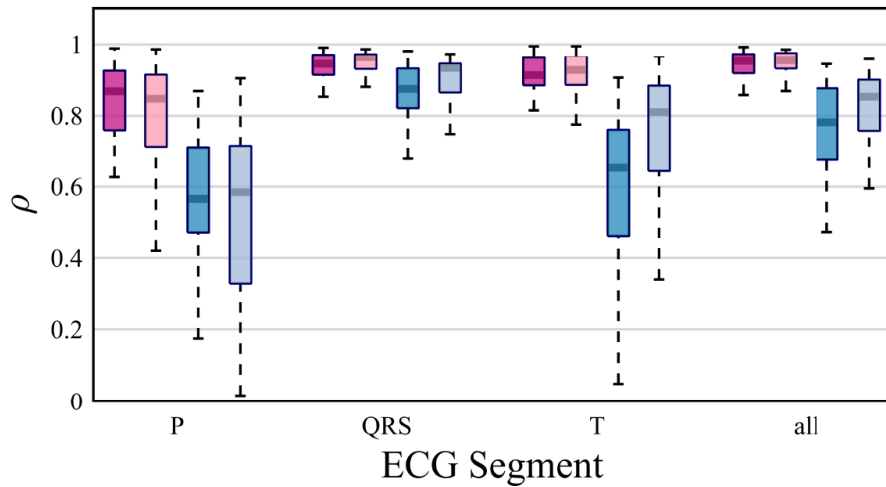


# Evaluation on Dataset 3: Mini-MIMIC III

Overall performance:

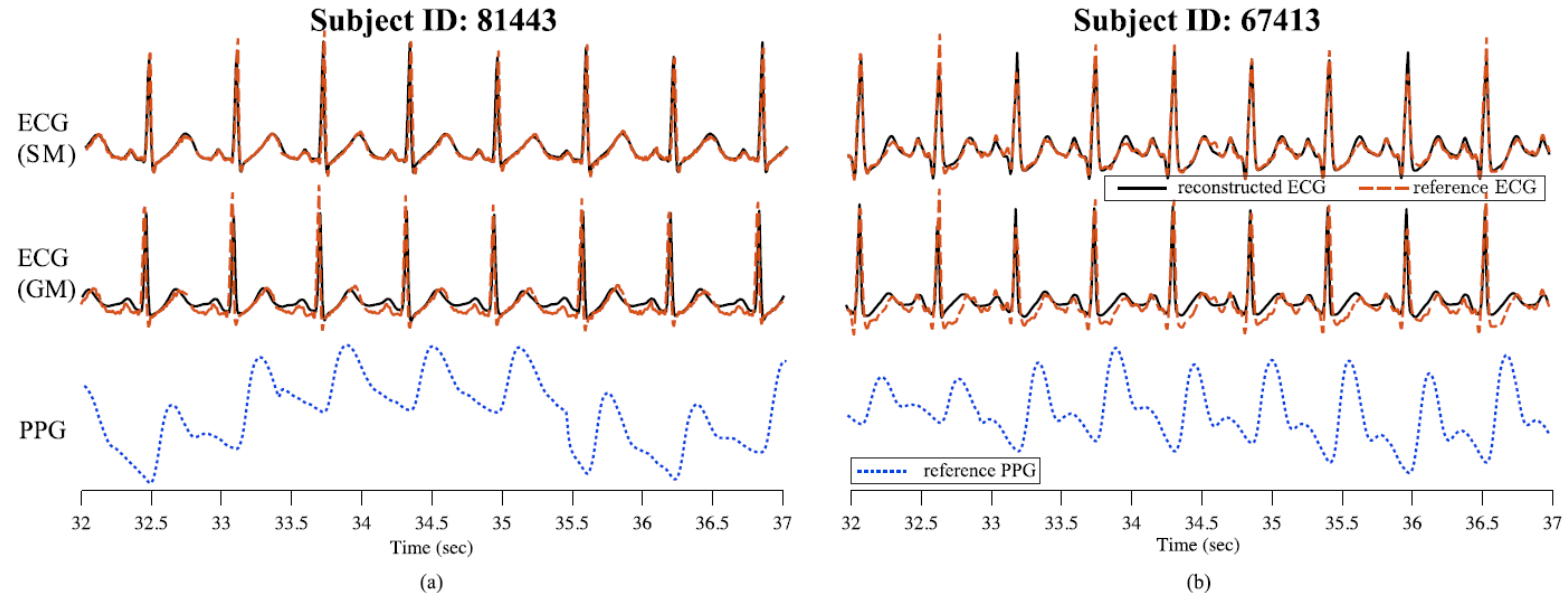


(a)



(b)

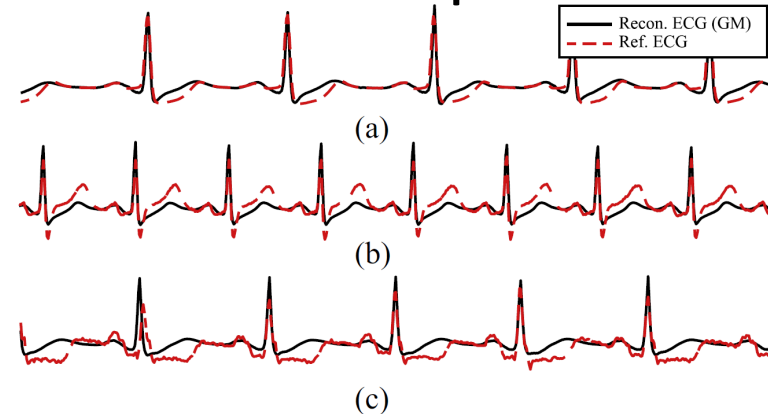
Good examples:



(a)

(b)

“low performance” examples:



(a)

(b)

(c)

# Cardio Disease Classification (subset from Mini-MIMIC III)

Confusion matrices & classification accuracy of SVM (w/ polynomial kernel) on ...

**Ori. ECG (ref.)**

**Recon. ECG (Proposed)**

**Ori. PPG**

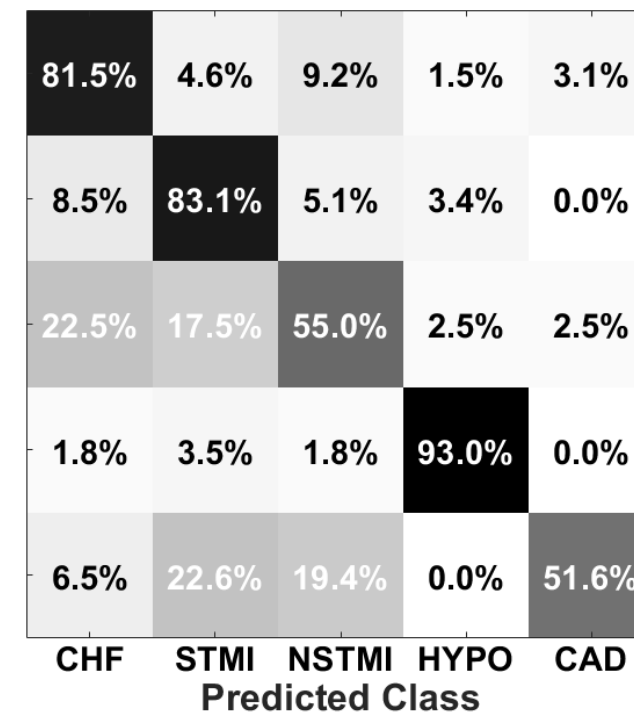
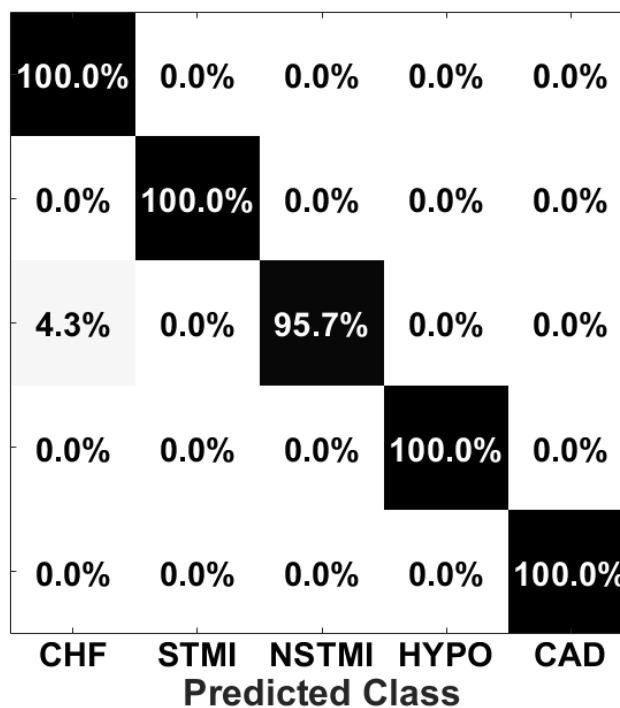
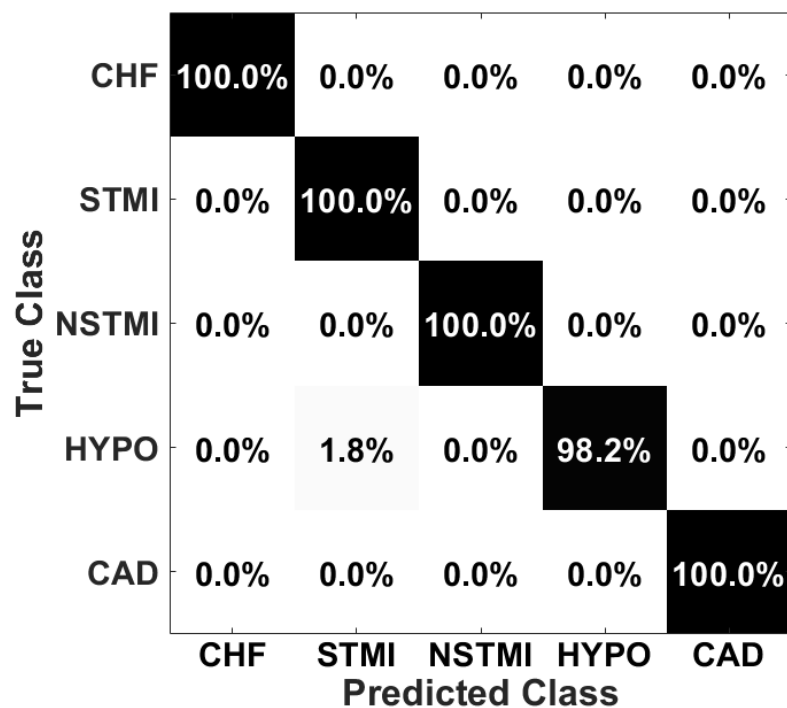
Accuracy:

99.6%

99.3%

76.6%

Confusion matrix from number of PCs = 100





# Conclusion

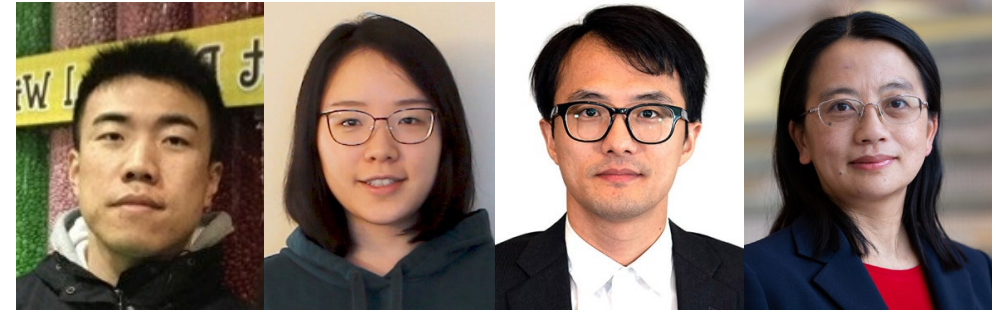
---

- Proposed and justified a **physiological model** to mathematically characterize the relationship between the ECG and PPG time-series signals using electrical, biomechanical, and optophysiological principles;
- Developed a **principled learning framework** based on the proposed physiological model and achieved encouraging accuracy of ECG reconstruction;
- Suggested an encouraging potential for a more **user-friendly, low-cost, continuous, and long-term cardiac monitoring** that supports and promotes public health, especially for people with special needs;
- Open a new direction to leverage a rich body of clinical ECG knowledge and transfer the understanding to **enrich the knowledge base for PPG** or other data from wearable devices.



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**icassp 2022**  
*Singapore*

# Learning Your Heart Actions From Pulse: ECG Waveform Reconstruction From PPG

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